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Research Article

### Evaluation of Two Populations of Equine Stem Cells in Promotion of Bone Healing in a Nude Rat Fracture Model

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#### Abstract

Equine bone marrow (BM) derived mesenchymal stem cells (MSC) have been used as a potential cell-based therapy in bone healing due to their osteogenic differentiation capacity. In this tibia fracture model in nude rats, the new bone formation was evaluated using a cell-based treatment with either fractionated or heterogeneous population of equine BM MSC in combination with Fibrin Glue (FG). Sternal equine BM MSCs were obtained from a donor horse and expanded *in vitro*. Stimulation of osteogenic differentiation of equine BM MSC was performed *in vitro* after cell incubation with osteogenic medium. Osteotomized tibias were treated with FG (Group 1), fractionated equine BM MSC combined with FG (Group 2), and heterogeneous cell population of equine BM MSC combined with FG (Group 3). Bone density, area of new bone formation and histology were evaluated 4 weeks after the surgery and treatment. Tibia fractures treated with a heterogeneous cell population of equine BM MSC and FG (Group 3) showed better callus formation, higher bone density and histology score as compared with rats treated with fractionated equine BM MSC in FG (Group 2) and FG alone (Group 1). A heterogeneous cell population of equine BM MSC could be a better cell-based therapy choice for bone healing in horse fractures.

**Keywords:** Horse; Mesenchymal Stem Cells; Bone Marrow; Nude rat; Osteotomy

## Introduction

Skeletal injuries in horses including bone fractures are a common clinical problem for equine orthopedic surgeons. Different surgical procedures have been used for improving bone fracture healing including autografts, allografts and implantation of implants [1]. The gold standard procedure is the implantation of autogenous bone graft which has osteogenic, osteoinductive and osteoconductive properties [2, 3]. However, limitations of this technique include the fact that harvest of bone graft may cause additional musculoskeletal pain, and the cost of such surgical procedures can be high with limited graft material availability [4, 5]. Tissue engineering approaches based in cell based therapy are an emerging option for delivering cells, growth factors, and extracellular matrix components or scaffolds in the site of bone fractures in order to improve and/or speed up the bone healing. Mesenchymal stem cells (MSC) from different types of tissues have shown the potential capability to differentiate into specific cell types under proper stimuli. It has been shown that bone marrow (BM) derived MSCs have the potential to differentiate into cells of the osteoblastic lineage and have been studied for use in regeneration of bone [6-14]. The osteogenic differentiation of BM derived MSCs has been shown *in vitro* with or without collagen scaffold [15]. In our laboratory, we have shown equine BM MSCs produce new bone after intramuscular implantation in nude mice [16].

While bone tissue engineering results have been promising, there is continued MSC characterization which focuses on identifying the best tissue source of MSCs for specific treatment based on the cellular morphology, presence of CD markers and stemness gene expression [17, 18]. A previous study has shown that equine muscle and BM MSCs have better osteogenic capacity compared with MSCs from periosteum and adipose tissue [19]. It is well known that as a primary culture, MSCs are a heterogeneous cell population [18, 20]. MSC subpopulations have shown different characteristics based on their morphology, proliferation, and differentiation abilities [21, 22]. In addition, the identification of a specific BM MSC subpopulation with the best osteogenic differentiation *in vitro* has been determined using a non-equilibrium gravitational field-flow fractionator (Flow s.r.l, Bologna, Italy). It has been suggested that an equine BM MSC fraction or subpopulation with ideal osteogenic differentiation may be valuable in cell-based therapy for bone healing in horses [23].

This study was intended to compare the osteogenic capacity and improvement in bone fracture healing amongst 3 groups (a heterogeneous cell population of equine BM MSCs; a purified, fractionated, equine BM MSC subpopulation; and control). Both BM MSC sources were combined with fibrin glue as a treatment in a rat tibia osteotomy experimental model. We hypothesized that a fractionated equine BM MSC subpopulation with optimum *in vitro* osteogenic differentiation capacity would improve the bone healing to a greater extent compared to a heterogeneous cell population of equine BM MSC and compared to a control.

## Methodology

All animal study protocols were approved by the University of Prince Edward Island Animal Care Committee.

### Animals

#### Rats

Twenty-four 9-week-old male NIH nude rats, with an average weight range of 233 +/- 4.16 grams were used in the study (Charles River Laboratories, Sherbrook, QC, Canada). Rats were housed as one rat per cage with a 12-hour light cycle. Food and water were provided *ad libitum*. Rats were randomly divided into two treatment groups (n=8 each) and one control group (n=8).

#### Horse

One horse was used for bone marrow collection. The horse was donated to the Atlantic Veterinary College for reasons independent to this study and determined to be systemically healthy based on physical examination, CBC, and chemistry panel. The horse was sedated with xylazine hydrochloride (1.1 mg/kg, IV) and euthanized with pentobarbital (108 mg/kg IV). Bone marrow aspirate was obtained aseptically immediately post mortem from the sternum with a bone marrow biopsy needle. The aspirate was collected into a 20ml syringe containing 2.5 ml heparin (1000 U/ml) and transported to the laboratory.

### Cell Isolation

Cells were isolated from BM using a centrifuge gradient technique and maintained in standard medium, as previously described [19]. Briefly, the samples were centrifuged at 1500 g for 10 minutes, then buffy coat was collected and placed in 75 cm<sup>2</sup> flasks with standard medium (SM) [(Dulbecco's Modified Eagle Medium (DMEM) Sigma Aldrich, St. Louis, MO), 10% fetal bovine serum (FBS) (PAA, Laboratories Inc. Etobicoke ON, Canada), 100 µg/mL penicillin (Sigma Aldrich, St Louis, MO), 50 µg/mL gentamicin sulphate (Sigma Aldrich, St Louis, MO), and 0.3 µg/mL amphotericin B (Invitrogen, Toronto, ON, Canada)]. Cultures were maintained in a humidified 5% CO<sub>2</sub> and 95% air atmosphere incubator at 37°C. Once cells adhered in 24-48 hours, unattached cells were washed off the flask with PBS. Medium was changed three times per week. Cells were maintained until 85% confluence. These cells were used as heterogeneous cell population of equine BM MSC treatment.

### Preparation of Fractionated BM MSC for Treatment

#### Cell Fractionation-Gravitational Field-Flow Fractionation (Gr-FFF)

A heterogeneous cell population of equine BM MSCs was washed with PBS and detached with 1 part trypsin (Invitrogen, Toronto, ON) and 4 parts Cellstripper solution (Corning, Manassas, VA). After 10 minutes of incubation at 37°C, the reaction was stopped with SM. Cell suspension

was spun at 1500 g for 10 min and counted. BM MSCs were aliquoted in  $5 \times 10^5$  cells in 50  $\mu$ l mobile solution (1g bovine serum albumin in PBS). Each aliquot was injected into a Gr-FFF system (Flow s.r.l, Bologna, Italy) with a 100  $\mu$ l micro syringe (Hamilton, Com., Reno, NV.) and sorted in 5 fractions by changing the collection tube every 5 minutes (0.5 ml per minute). Equine BM MSC fractions were incubated in SM at 37°C in a humidified 5% CO<sub>2</sub> and 95% air atmosphere. Fraction 4 was cryopreserved for further propagation and used for cell-based treatment.

### Fibrin Glue Preparation

Two donor horses, 5 and 15 years old, that were not enrolled in the study, were used for collection of blood which was used for making a fibrin glue (FG) scaffold. Fibrin glue was produced using a cryoprecipitation technique as described by Dresdale [24]. Briefly, plasma was divided in 50 mL polypropylene centrifuge tubes (BD Falcon, Franklin Lakes, NJ) and placed in a freezer at -80°C for 12 hours. Then, tubes were slow thawed at 4°C. After thawing, tubes were centrifuged at 1000 g for 15 minutes, supernatant was decanted and saved for further use, leaving a yellowish precipitate of fibrinogen. Fibrinogen concentration was measured and diluted with the supernatant at a final concentration of 50 mg/mL.

### Scaffold Preparation and Osteogenic Differentiation

Five million equine BM MSCs from the heterogenous cell population were mixed with 75  $\mu$ L of fibrin and 75  $\mu$ L of thrombin, diluted in 40nM CaCl<sub>2</sub> (Sigma Aldrich, Canada Ltd., Oakville, ON, Canada), to obtain a final concentration of 250 U/mL. Five million of fractioned equine BM MSC was mixed with FG as previously described. Fibrin glue without MSCs was prepared mixing fibrin and thrombin only. Mesenchymal stem cells and FG scaffolds were supplemented and incubated with osteogenic media (OM) [ $\alpha$ -MEM, 5% FBS, 100  $\mu$ g/mL penicillin, 50  $\mu$ g/mL gentamicin sulfate, 0.3  $\mu$ g/mL amphotericin B, 50  $\mu$ g/mL ascorbic acid (Sigma Aldrich, St. Louis, MO),  $10^{-8}$  M dexamethasone (Sigma Aldrich, St Louis, MO), and 10 mM,  $\beta$ -glycerophosphate (Sigma Aldrich, St Louis, MO)] to stimulate osteogenic differentiation for 48 hours prior to surgical implantation.

### In Vivo Experiment

#### Surgical Procedure

Rats were maintained in a sterile environment in the laboratory animal facility for the duration of the study. Rats were anaesthetized with 2% isoflourane (Pharmaceutica Partners of Canada Inc. ON, Canada), placed in dorsal recumbency, and aseptically prepped. Pre-operative treatment for each rat consisted of 3 mL of subcutaneous (SC) fluids (Lactate Ringers solution Baxter, Mississauga On), buprenorphine 0.05mg/kg SC (Vetergesic, Alstoe Ltd., Sheriff Hutton, York, UK), enrofloxacin (10 mg/kg SC) and eyes were covered with sterile ophthalmic liquid gel (Tear-gel Novartis, Dorval, QC, Canada).

Surgery was conducted using routine aseptic techniques. The left tibia and stifle were clipped and aseptically prepped. The rat was draped and the distal aspect of the tibia tuberosity was palpated as a landmark. A 1-cm incision was made through the skin and periosteum starting at the distal aspect of the tibia tuberosity and extending distally over the medial aspect of the left tibia. One centimeter of periosteum was elevated off the tibia diaphysis. The osteotomy was made in the center of this area (5 mm distal to the distal end of the tibia tuberosity). The bone was lavaged with saline, and the bone was cut with an oscillating saw using a small sagittal blade (ConMed Linvatec., Largo, FL). A 0.035-inch diameter K-Wire (IMEX Veterinary Inc., Longview, TX.) was used to stabilize the fracture. The pin was placed retrograde. One centimetre of pin was placed in the distal aspect of the tibia beyond the osteotomy site. The pin was cut at the proximal end. Rats were randomly assigned to a treatment group. Treatment groups were as follows (n=8): *Group 1.* FG; *Group 2.* Fractioned equine BM MSCs in FG; *Group 3.* Heterogeneous cell population of equine BM MSCs in FG. The randomly assigned treatment (group 1, 2, and 3) was implanted at the osteotomy site after stabilization of the fracture. Muscles were sutured with 4(0) polydioxone (PDS II, Ethicon Inc., Somerville, NJ). The skin incision was glued using GLUture (Abbott laboratories Ltd., Berkshire, UK). Rats were maintained with food and water *ad libitum*, and monitored daily for the remaining 4 weeks of the study. Rats were administered meloxicam per os 2mg/kg (Metacam, Boehringer Ingelheim, Burlington, ON, Canada) daily for one week. Enrofloxacin (0.1 mg/ml) and buprenorphine B (0.0006 mg/ml) were dissolved in water and provided *ad libitum* for one week. Post-operative monitoring of the rats included evaluation of the attitude and use of the limb each day when medication was administered, as well as weight assessment once a week. Rats were euthanized with CO<sub>2</sub> 4 weeks post-surgery.

### Radiography

Radiographic images of the hind limbs were taken immediately post mortem after 4 weeks from treatment and surgery using Provetra V digital imaging (AllPro Imaging, Melville, NY). Objective bone density data was obtained for each hind limb using an image analysis system (Image J, National Institutes of Health, Bethesda, MD; <http://imagej.nih.gov/ij/>, 1997–2011).

### Histology

At the 4-week endpoint, all left tibias were dissected and fixed in buffered formalin for 24 hours. Then tibias were demineralized in constant stir for 24 hours in a solution containing 120ml formic acid, 24g sodium formate in one liter of deionized water. After demineralization, tibias were placed in 70% ethanol for 48 hours. Tibias were paraffin-embedded and cut into 5  $\mu$ m sections and stained with H & E. Three of the authors evaluated the tissue sections in a blinded manner. Presence or absence of cartilage, bone, condensed mesenchyme, or normal muscle tissues were recorded for H and E stained sections (two sections per

sample) [25-27] (Table 1). When new bone was identified, image analysis was used to quantify the area of new bone for comparison among groups using an image analysis system (Image J, National Institutes of Health, Bethesda, MD; <http://imagej.nih.gov/ij/>, 1997–2011).

Score/Grade	Bone Healing Stage
0	Non union (fibrous tissues)
1	Incomplete cartilage union (cartilage with some fibrous tissue)
2	Complete cartilage union (entirely cartilage)
3	Incomplete bone union with early ossification phase (predominantly cartilage with some trabecular bone)
4	Incomplete bony union with late ossification phase (equal amounts of cartilage and trabecular bone)
5	Incomplete bony union with late ossification phase (predominantly trabecular bone with some cartilage)
6	Complete bony union (entirely bone)

**Table 1.** Scale Grading for Bone Healing

### Statistical Analysis

The results of quantitative analysis are reported as the mean ( $\pm$  SD) Kruskal-Wallis test was used to compare the differences between groups, and a post-hoc analysis was performed with Mann-Whitney U test. Statistical analyses were performed using IBM SPSS Statistics 21 software. Statistical significance was set at  $P < 0.05$ .

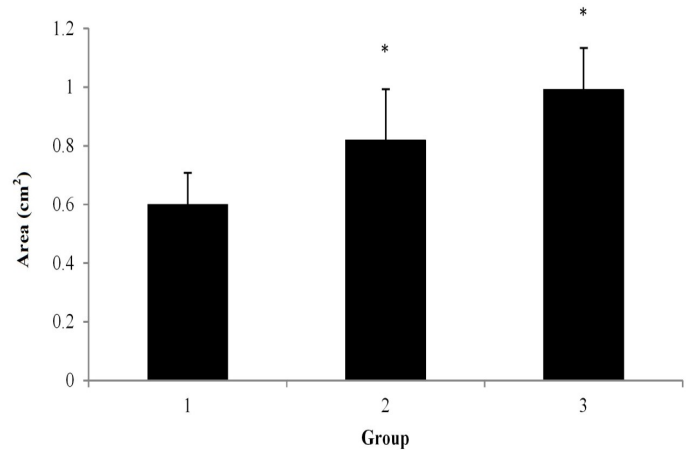
### Results

#### Area of New Bone Formation

The area of the endochondral ossification in the tibia osteotomies was measured from H & E histological sections performed 4 weeks after surgery and treatment. Tibial fractures treated with fractioned equine BM MSCs and heterogeneous cell population of equine BM MSCs (Groups 2 and 3, respectively) showed a significant increased area of endochondral ossification ( $P < 0.05$ ) in the osteotomy sites, as compared with tibia osteotomies treated with FG only (Group 1). No statistical difference was observed between tibia fractures treated with fractioned equine BM MSCs and heterogeneous cell population of equine BM MSCs (Groups 2 and 3) (Figure 1).

#### Radiographic Analysis and Bone Density

New bone or callus formation was evident in rats 4 weeks after surgery and treatment. Control group rats showed less callus formation at the tibia osteotomy treated with FG only (Group 1) (Figure 2A).



**Figure 1.** An increased area of new bone formation was evident in rats treated with fractioned equine BM MSCs (Group 2) and heterogeneous cell population of equine BM MSCs (Group 3). Compared to the control group ( $P < 0.05$ ) (Group 1).

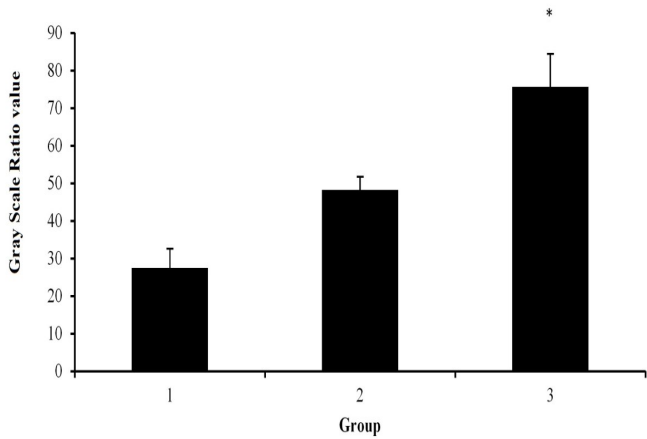


**Figure 2.** Representative radiographic images of rat tibias osteotomies treated with FG (A), fractioned equine BM MSCs (B) and heterogeneous cell population of equine BM MSCs (C).

Therefore, no established bone union was observed in this group. In the group of rats treated with fractioned equine BM MSCs (Group 2) more callus formation was observed at the tibia osteotomy. This space was partially filled with callus formation (Figure 2B). In the group of rats treated with heterogeneous cell population of equine BM MSCs (Group 3), the osteotomy site was covered by callus formation, representing bone union (Figure 2C). Results from radiological density at 4 weeks showed higher bone density in rats treated with heterogeneous cell population of equine BM MSC ( $P < 0.05$ ) (Group 3), as compared with rats treated with fractioned equine BM MSCs (Group 2) and control group treated with FG only (Group 1) (Figure 3).

#### Histology Score

Histology assessment of tibia osteotomy of rats treated with FG (Group 1) showed nonunion bone, or incomplete cartilage union with fibrous tissue (Figure 4A). Tibia osteotomy sections from rats treated with fractioned equine BM MSCs (Group 2) showed incomplete bone union

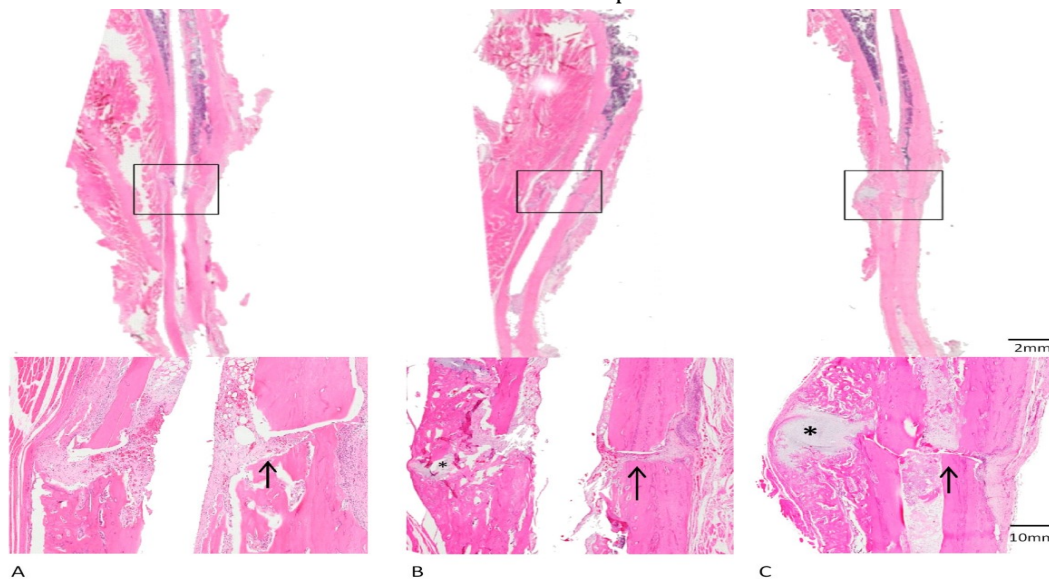


**Figure 3.** Gray scale ratio values representing bone density was significantly greater ( $P<0.05$ ) in rats treated with a heterogeneous cell population of equine BM MSCs (Group 3) as compared with rats treated with fractionated equine BM MSCs (Group 2) and control group (FG) (Group 1).

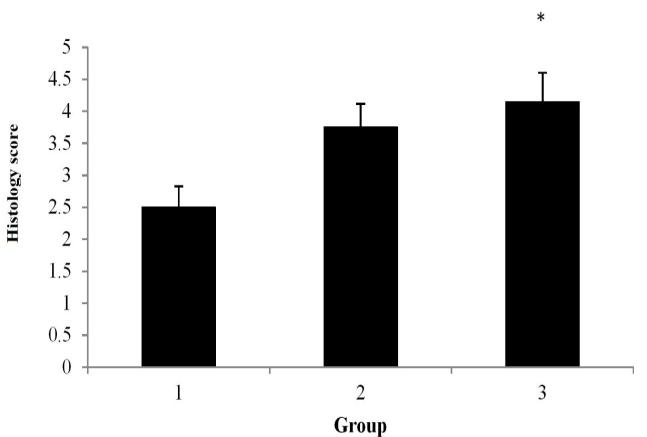
with similar amounts of cartilage and trabecular bone (Figure 4B). Histology sections from rats treated with a heterogeneous cell population of equine BM MSCs (Group 3) showed incomplete or complete bony union predominantly composed of trabecular bone and small amounts of cartilage (Figure 4C). Histology score analysis from the three groups showed a significantly higher score of new bone formation in rats treated with heterogeneous cell population of equine BM MSCs (Group 3) as compared with rats treated with FG and fractionated equine BM MSCs (Group 1 and 2 respectively) (Figure 5).

**Discussion**

The present study demonstrated that a locally applied osteogenic, primed, heterogeneous cell population of equine BM MSCs mixed in a fibrin glue scaffold improved the bone healing in a tibia fracture model in nude rats compared with fractionated equine BM MSCs in FG and control group (FG). Cell based treatment in this experiment was selected based on previous *in vitro* and *in vivo* characterization of equine



**Figure 4.** Representative histology micro-sections stained with H & E from rat tibias treated with FG (Group 1), fractionated equine BM MSC (Group 2), and heterogeneous cell population of equine BM MSC (Group 3). Rectangle in top images is showed in amplified bottom images. Arrows indicate the bony union site. Asterisks indicate presence of newly cartilage.



**Figure 5.** Histology score from rat tibia osteotomies treated with a heterogeneous cell population of equine BM MSCs (Group 3) showed significantly higher ( $P<0.05$ ) new bone formation compared with rats treated with fractionated equine BM MSCs (Group 2) and FG (Group 1).

BM MSCs in our laboratory [15, 19, 23, 28]. Those results showed a higher: osteogenic gene expression in equine BM MSC stimulated with osteogenic medium; osteogenic differentiation in different types of scaffolds; and heterotopic new bone formation in nude mice and rats compared to MSCs derived from other equine tissues. In addition, we evaluated the osteogenic differentiation of equine BM MSCs sorted into subpopulations by gravitational field-flow fractionation. Equine subpopulations of BM MSCs showed different osteogenic gene expression *in vitro*, between sorted fractions. Of cell subpopulations, fraction 4 showed the highest osteogenic gene expression [23, 29]. Thus, this cell fraction was selected as a cell-based treatment in this animal fracture model experiment. Equine MSC fractionation has been reported using FACS as a lab technique to identify stemness characteristics [18] as well as sieved-size subpopulations from equine umbilical cord [20]. In addition, enriched and purified human BM MSC CD34+

showed increased vascularisation and bone formation in a femur fracture model in nude rats [27].

Results from this experiment demonstrated that a heterogeneous cell population of equine BM MSCs combined with FG resulted in better bone healing of the fractured tibias compared with fractioned equine BM MSCs in FG. Scaffolds and cell carriers are one of the most important issues in tissue engineering. Particularly, FG has been shown to be an excellent carrier/scaffold [30] which allows cell survival and differentiation [15]. Overall, the benefit of FG in bone healing has been reported in human and animal models through the induced new bone formation when combined with stem cells and demineralized bone [30]. In addition, FG has shown osteoinductive properties when implanted in the extra skeletal site of mice and human as a potential biologic tissue adhesive [33, 34]. Previous results from *in vivo* experiments in our laboratory demonstrated new bone formation with heterotropic injection of equine BM MSCs in FG. New bone formation did not occur when equine muscle derived MSCs in FG were injected in the same model [16]. Similar results were observed in other laboratories. In nude mice subcutaneously implanted with equine BM MSCs and FG, there was increased vascularisation and tissue repair compared with FG alone [31, 32]. In addition, *in vitro* experiments have shown that equine BM MSCs had better osteogenic differentiation in FG and in collagen type I carriers as compared with monomeric collagen and rat tail collagen [15].

Our histologic evaluation from tibia fractures treated with the heterogeneous cell population of equine BM MSCs combined with FG showed better histology score, presence of callus, and new bone formation compared with fractioned equine BM MSCs combined with FG. Equine BM MSCs have been shown to have better osteogenic capacity *in vitro* when combined with FG and collagen type I scaffolds [15] compared to equine MSCs derived from other tissues. In spite of few reports using equine BM MSCs in bone repair in live animal models, there are publications regarding the potential use of BM MSCs from different animal species in calvarial defects, experimental polytrauma and hemorrhagic shock, femur fracture, mandible and alveolar defects, and osteoporosis [15, 35-40].

There are few reports regarding the use of equine MSCs in equine fractures, and these reports showed variable results [41, 42]. Periosteal-derived stem cells did not improve the bone healing in a horse osteotomy model [41]. Whereas, in a mouse heterotopic model, of BM derived equine MSCs showed new bone formation and mineralization [16]. In an equine metatarsal bone defect model, equine BM MSCs stimulated the bone formation only with the addition of bone marrow morphogenetic protein-2 [42].

It has been shown that osteogenic gene expression is different in fractioned equine BM MSC [23]. However, fractioned equine BM MSCs with the highest osteogenic gene expression [fraction 4, 23] did not result in better bone repair in this tibia fracture model. Those fractioned equine BM MSCs with lower *in vitro* osteogenic gene expression

may have a role in the extracellular matrix production and/or in the production of growth factors which are required for bone remodeling. Further studies, such as proteomic profile are necessary to understand the molecular mechanisms of osteogenic differentiation of equine MSCs.

In conclusion, tibia fractures treated with a whole population of equine BM MSCs showed better bone healing compared with a subpopulation of equine BM MSCs. Although there is evidence of the successful use of MSCs in bone repair of animal models, more studies are necessary to identify the best source of MSCs with osteogenic capacity, as well as the best *in vitro* culture conditions. As there are only few reports using MSCs in equine bone repair, more clinical studies are required to demonstrate the feasibility of the MSC based therapy as a potential choice in the treatment of bone fractures in horses.

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